Network dissimilarity measure and application to brain network differentiation

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- Motivation
- Dissimilarity measure
- Applications

Campus d'Excel·lència Internacional

Motivation: how to compare time-evolving correlation networks



Example: desertification transition under the lens of correlation network



G. Tirabassi et al., Ecological Complexity (2014)

Network analysis

Degree (number of links of a node)

 Assortativity (average degree of the neighbors of a node)

 Clustering coefficient (fraction of neighbors of a node that are also neighbors among them)

$$c_i \equiv \frac{1}{k_i(k_i-1)} \sum_{j=1}^N \sum_{l=1}^N A_{ij} A_{jl} A_{li}$$



"Randomization" of the network when the tipping point is approached



The "randomization" can be quantified by the Kullback–Leibler Distance



$$\mathsf{KLD} \equiv \int_{-\infty}^{\infty} \ln\left(\frac{P(x)}{Z(x)}\right) P(x) \, \mathrm{d}x.$$

 Open issue: the "Gaussianisation" might be a modelspecific feature.

G. Tirabassi et al., Ecological Complexity 19, 148 (2014)

Other examples of time-evolving correlation networks







Climate





Weighted degree

Climate networks: how to detect relevant changes in the connectivity paths of the network?



Main Goal: to develop a measure that allows a precise comparison of complex networks (including different sizes)

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In order to detect structural changes we need a precise measure to compare networks

- Degree, centrality, assortativity distributions etc. provide partial information.
- How to define a measure that contains detailed information about the global topology of a network, in a compact way?
- \Rightarrow Node Distance Distributions (NDDs)
- p_i(j) of node "i" is the fraction of nodes that are connected to node i at distance j
- If a network has N nodes:

NDDs = vector of N pdfs { $p_1, p_2, ..., p_N$ }

If two networks have the same set of NDDs ⇒ they have the same diameter, average path length, etc.

How to condense the information contained in the node distance distributions?

- The Network Node Dispersion (NND) measures the heterogeneity of the N pdfs {p₁, p₂, ..., p_N}
- Quantifies the heterogeneity of connectivity distances.

$$NND(G) = \frac{\mathcal{J}(\mathbf{P}_1, \dots, \mathbf{P}_N)}{\log(d+1)} \quad d = \text{diameter}$$
$$\mathcal{J}(\mathbf{P}_1, \dots, \mathbf{P}_N) = \frac{1}{N} \sum_{i,j} p_i(j) \log\left(\frac{p_i(j)}{\mu_j}\right)$$
$$\mu_j = \left(\sum_{i=1}^N p_i(j)\right)/N$$

Example of application: in a random network the nodedistance-distribution detects the percolation transition



Dissimilarity between two networks

$$D(G, G') = w_1 \sqrt{\frac{\mathcal{J}(\mu_G, \mu_{G'})}{\log 2} + w_2} \left| \sqrt{\text{NND}(G)} - \sqrt{\text{NND}(G')} \right| \qquad w_1 = w_2 = 0.5$$

compares the co averaged he connectivity co

compares the heterogeneity of the connectivity distances

- Extensive numerical experiments demonstrate that isomorphic graphs return *D=0*.
- Computationally efficient.

Meaningful comparison of networks with the same number of nodes and links



Distances between real networks (Koblenz Network Collection)



Comparing real networks to null models

DS

preserves the degree sequence; **2.0** also preserves the degree correlation; 2.1 also the clustering coefficient; **2.5** also the clustering spectrum



Comparing brain networks

- EEG data
 - https://archive.ics.uci.edu/ml/datasets/eeg+database
 - 64 electrodes placed on the subject's scalp sampled at 256 Hz during 1s
 - 107 subjects: 39 control and 68 alcoholic
- Use Horizontal Visibility Graph to transform each EEG Time Series into a network.
- The HVG method is applied to the raw data (no prefiltering to extract a particular frequency band).

The horizontal visibility graph (HVG) method: transforms a time series into a unweighted and undirected graph



- Each data point is a node.
- <u>Rule</u>: data points *i* and *j* are connected if there is "visibility" between them (Xi and Xj > Xn for all n i<n<j)

Luque et al PRE (2009); Gomez Ravetti et al, PLOS one (2014)

Horizontal Visibility Graph

A time series



For each subject, the time series recorded at each electrode is transformed into a graph



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Dataset has 64 channels \Rightarrow 64 networks



The brain network of each subject

The weight of the link between two graphs (G, G') representing two brain regions is defined as: 1-D(G,G')



The resulting network (with 64 nodes=electrodes, all-to-all coupled with weighted links) represents the similarity between the EEG signals in different brain regions of one subject.
⇒ We can then compare different subjects.

We identify two brain regions (called 'nd' and 'y'), where the connection strength between these regions is higher in control than in alcoholic subjects.



Connection strength

Using the Hamming distance we can not distinguish.



T. A. Schieber et al, Nat. Comm. 8, 13928 (2017)

Retina image classification using node distance distribution Pablo Amil, ITN BE-OPTICAL, ongoing work in collaboration with Irene Sendiña, IRJC



The distance distribution of the central node: a promising classification tool



Another method to transform a time series into a graph: symbolic analysis



Ordinal patterns of 4 "letters"



Adapted from M. Small (The University of Western Australia)

U. Parlitz et al. / Computers in Biology and Medicine 42 (2012) 319-327

This method gives a weighted and directed graph

- D! nodes
- Weigh of node i: the probability of pattern i (∑_i p_i=1)
- Weight of the link i→j: probability of the transition i→j (for each *i*: ∑_j w_{ij}=1)



Measures used to characterize the graph

Entropy computed from node weights (permutation entropy)

$$s_p = -\sum p_i \log p_i$$

Average node entropy (entropy of the link weights)

$$s_n = \frac{1}{M} \sum_{i=1}^{M} s_i$$
 $s_i = -\sum_{j=1}^{M} w_{ij} \log w_{ij}$

Asymmetry coefficient: normalized difference of transition probabilities, $P('01' \rightarrow '10') - P('10' \rightarrow '01')$, etc.

$$a_{c} = \frac{\sum_{i} \sum_{j \neq i} \left| w_{ij} - w_{ji} \right|}{\sum_{i} \sum_{j \neq i} \left(w_{ij} + w_{ji} \right)}$$

(0 in a fully symmetric network;1 in a fully directed network)

Application: distinguishing eyes closed (EC) and eyes open (EO) brain states

Carlos Quintero ITN NETT, ongoing work in collaboration with A. Pons, M. C. Torrent, J. Garcia-Ojalvo and BitBrain.

	DTS1	DTS2
Sampling rate(Hz)	256	160
Time $task(seg)$	120	60
Total points	30720	9600
Number of electrodes	16	64
Number of subjects	70	109

BitBrain PhysioNet



 Symbolic analysis is applied to the raw data; similar results were found with filtered data using independent component analysis.

Permutation entropy and node entropy (PhysioNet)





"Randomization": the entropies increase and the asymmetry coefficient decreases



Time window = 1 s (160 data points)

Concluding

Summary

- New measure to quantify the heterogeneity of the connectivity paths of a single network.
 - detects the percolation transition in a random network.
- New measure to calculate distance between graphs
 - can be applied to graphs of different sizes.
 - returns *D*=0 only if they are isomorphic.
- Used to differentiate brain networks (alcoholic/non alcoholic) constructed using the horizontal visibility graph (raw EEG).
- Many possible applications for characterizing time-evolving networks, classification of biomedical data, etc.
- Symbolic analysis also applied to raw EEG data seems promising for differentiating brain states.



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http://www.fisica.edu.uy/~cris/

G. Tirabassi et al., Ecological Complexity 19, 148 (2014)

T. A. Schieber et al, Nat. Comm. 8, 13928 (2017)

